

A Template-free Pipeline for Recovering Structures in Cryo-electron tomography

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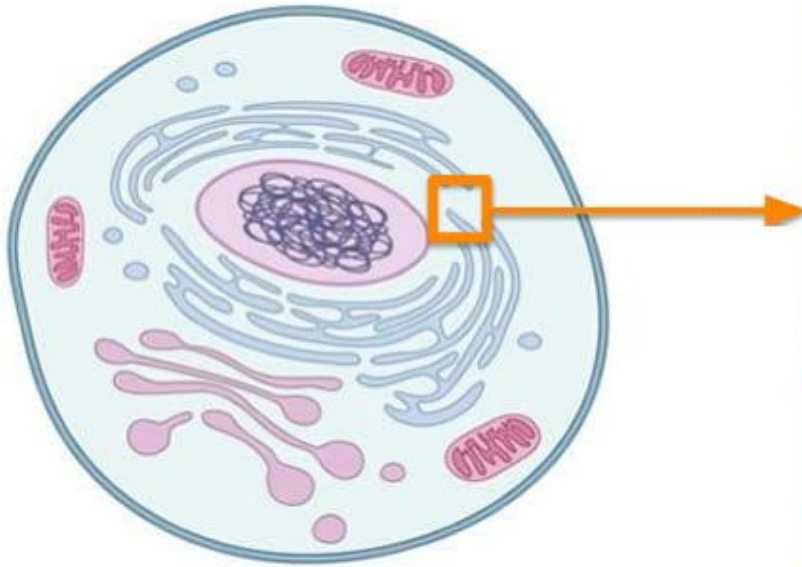
Computational Biology Department
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MMBioS Monthly Scientific Meeting

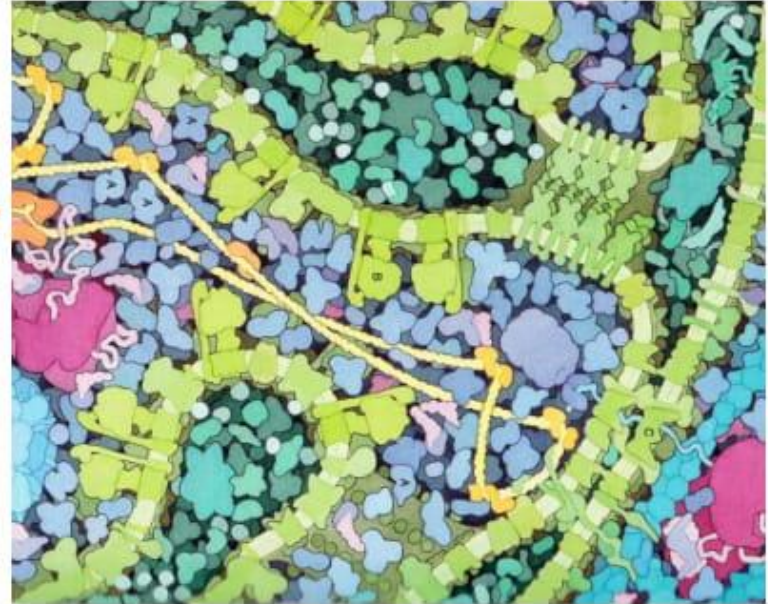
November 1, 2018 2:00-3:00 pm

Macromolecules

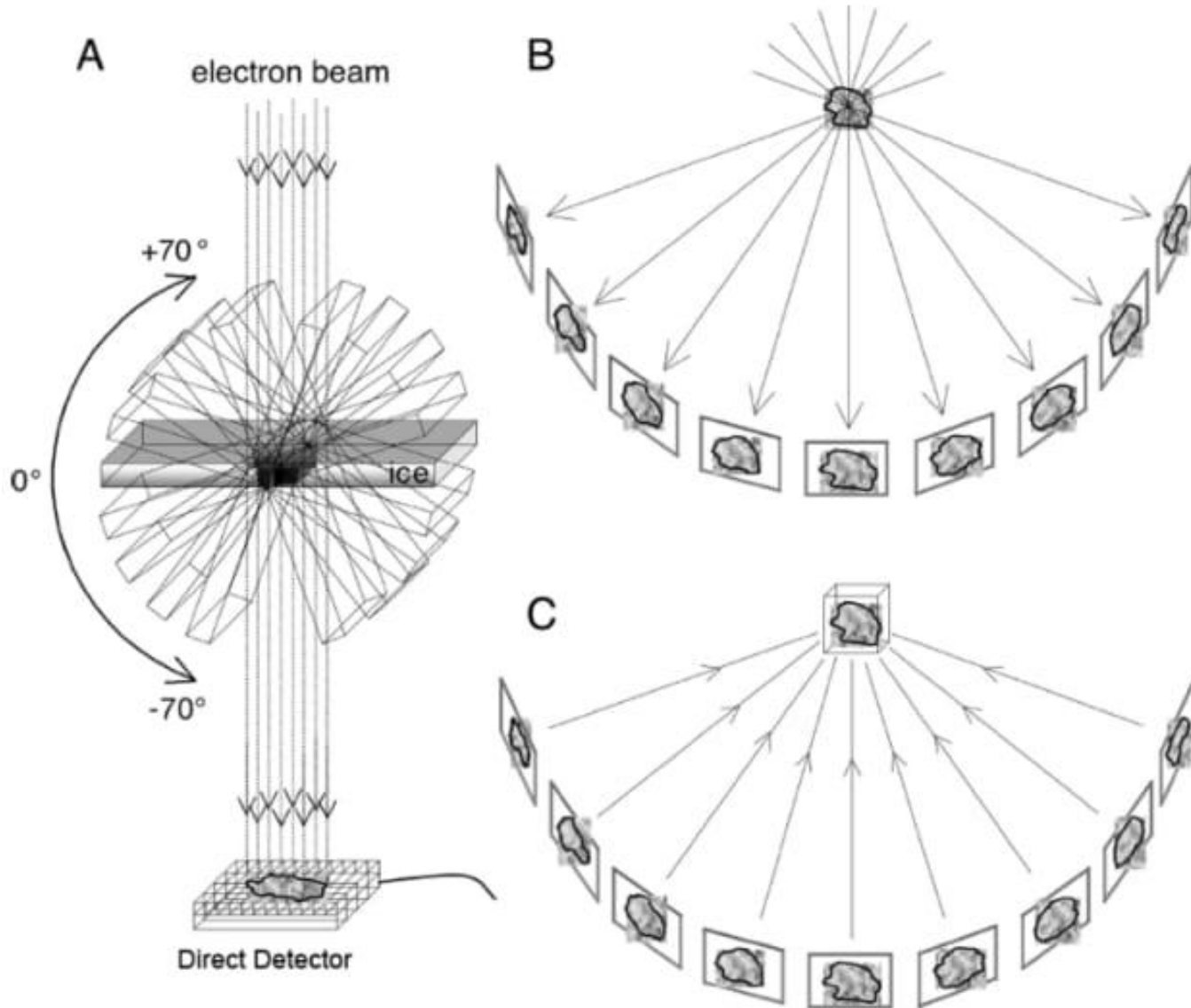
Cell



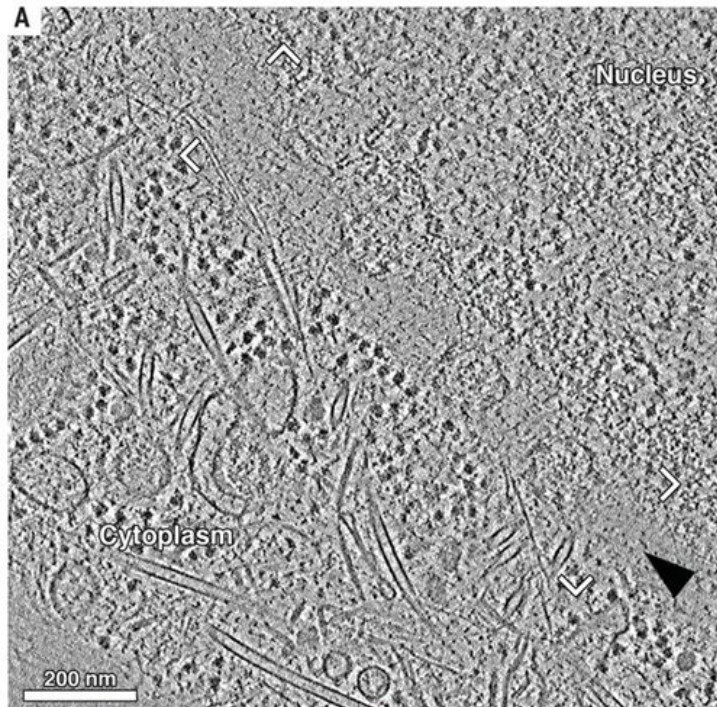
Cell cytoplasm



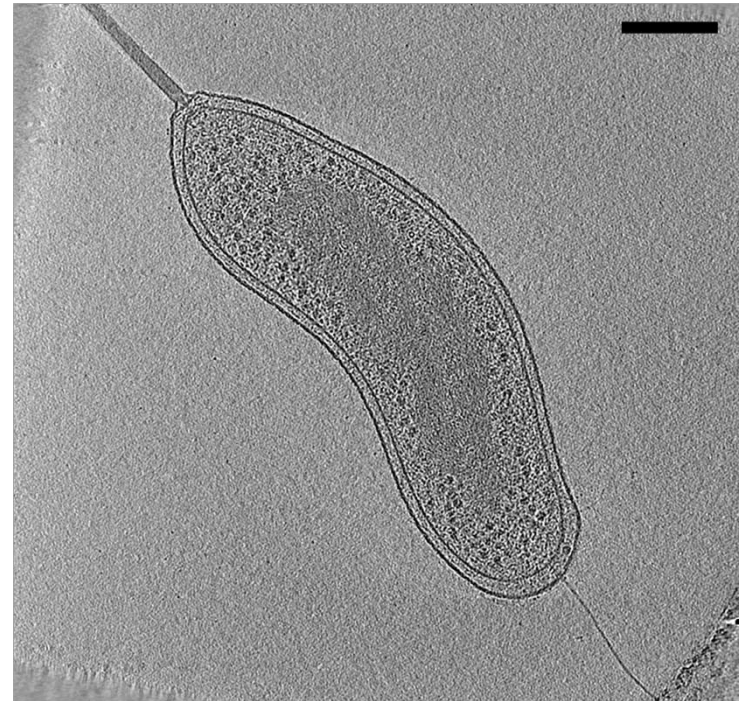
Tilt series and reconstruction



Example slices of 3D tomogram

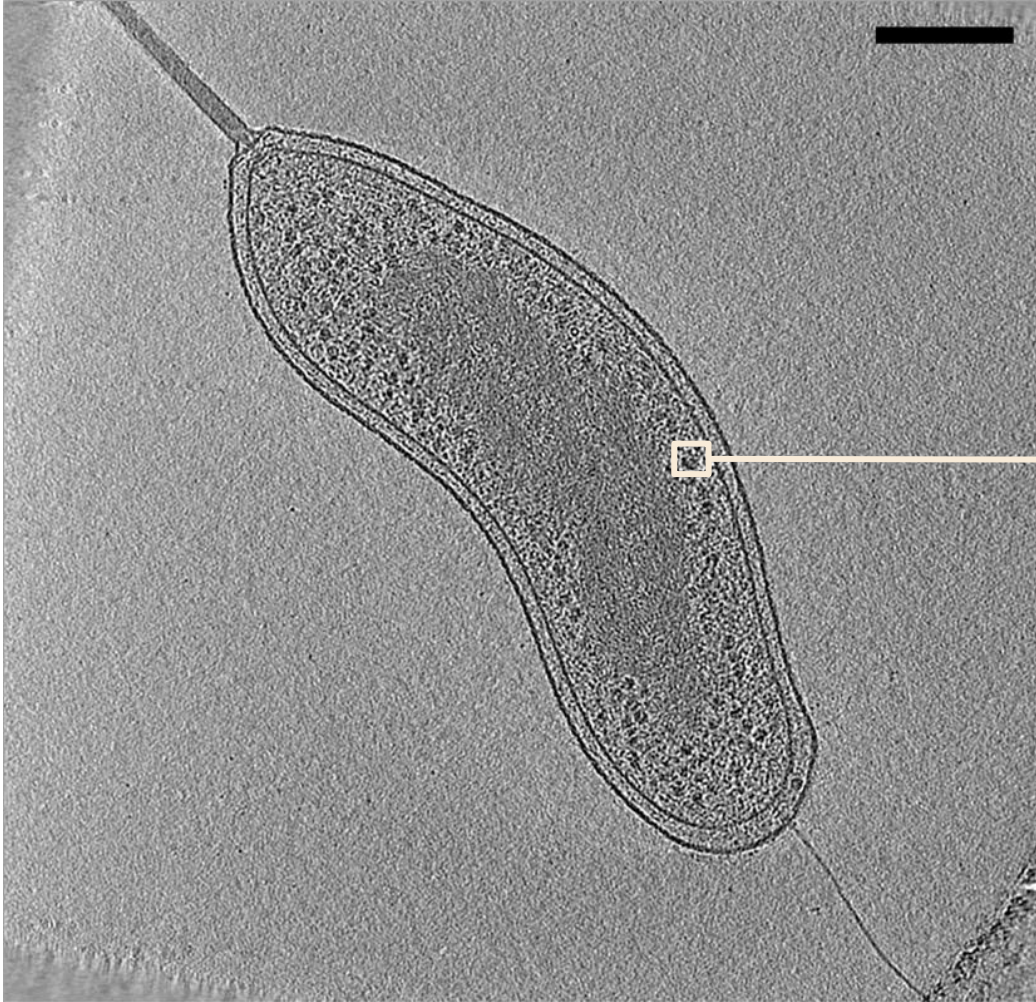


Mahamid et al, Science, 2016



Grant Jensen Lab at Caltech

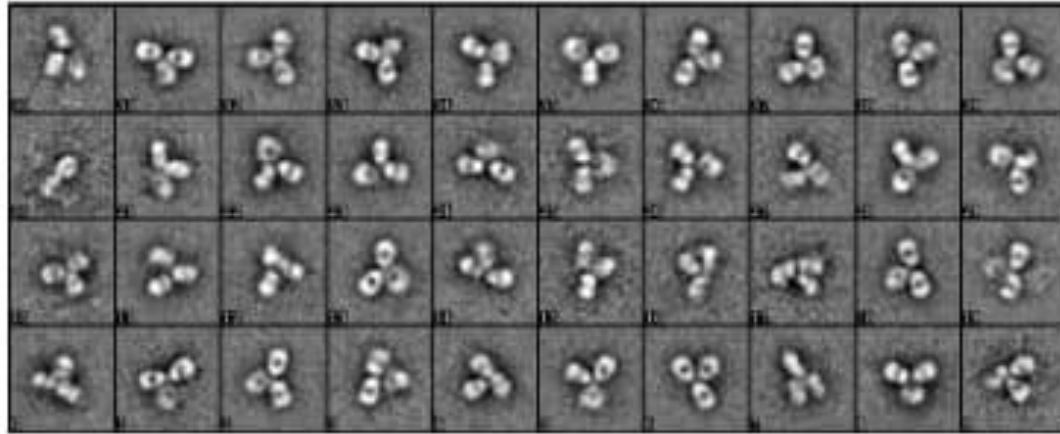
Subtomogram extraction



A subtomogram containing one macromolecule

Challenge 1: Orientation

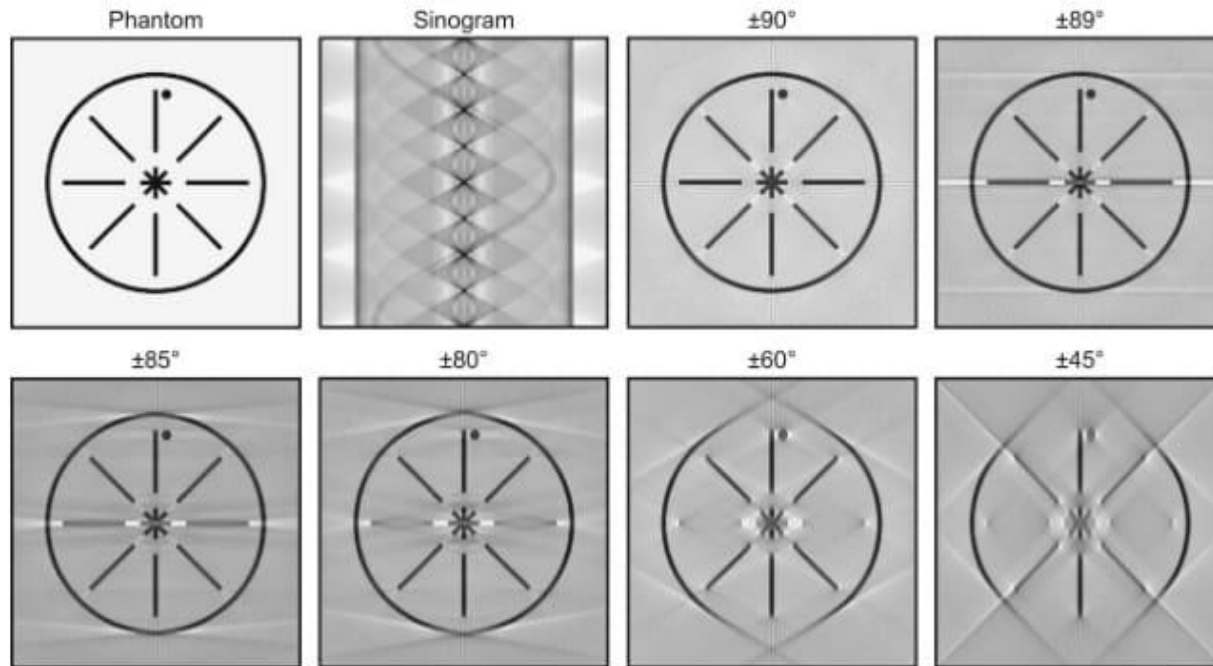
Particles can adopt all different orientations in 3D space



IgG antibodies

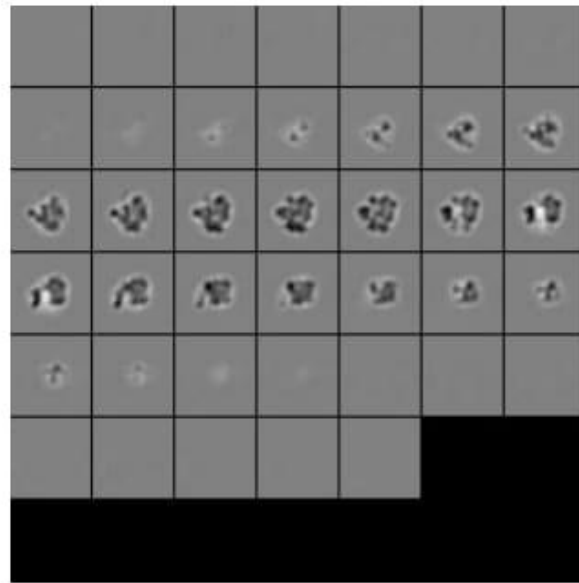
Challenges 2: Missing wedge effect

Reconstruction distortion due to limited range of tilt angles

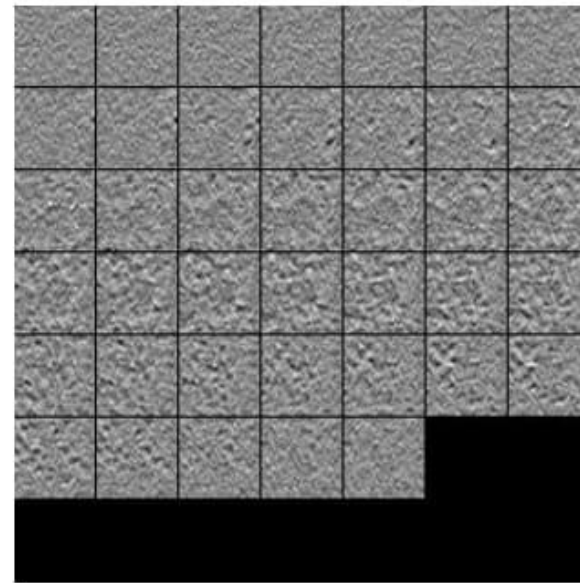


Challenges 3: Noise

Subtomograms are very noisy

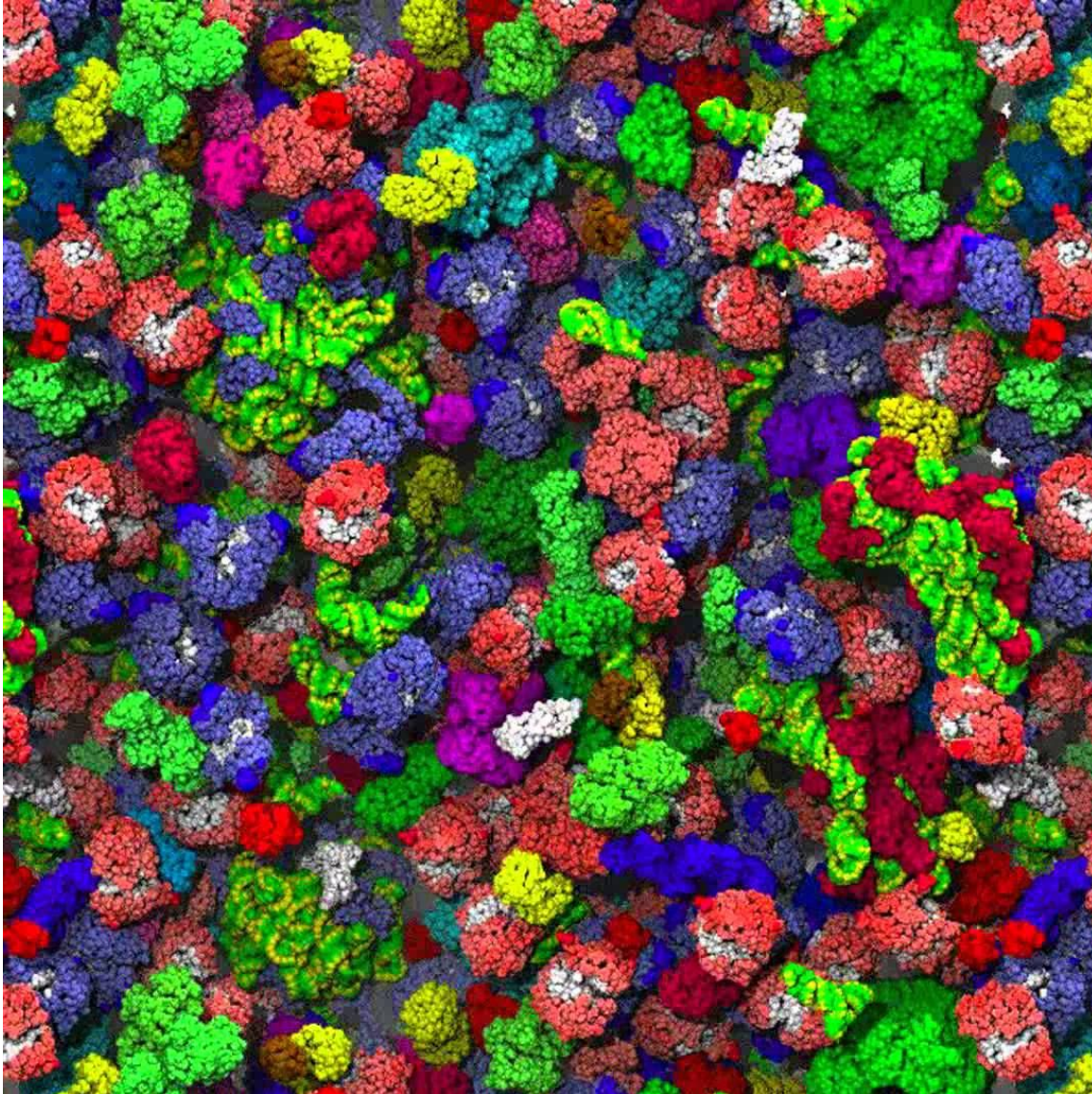


Mammalian ribosome
ground truth (40^3)



Mammalian ribosome
experimental data

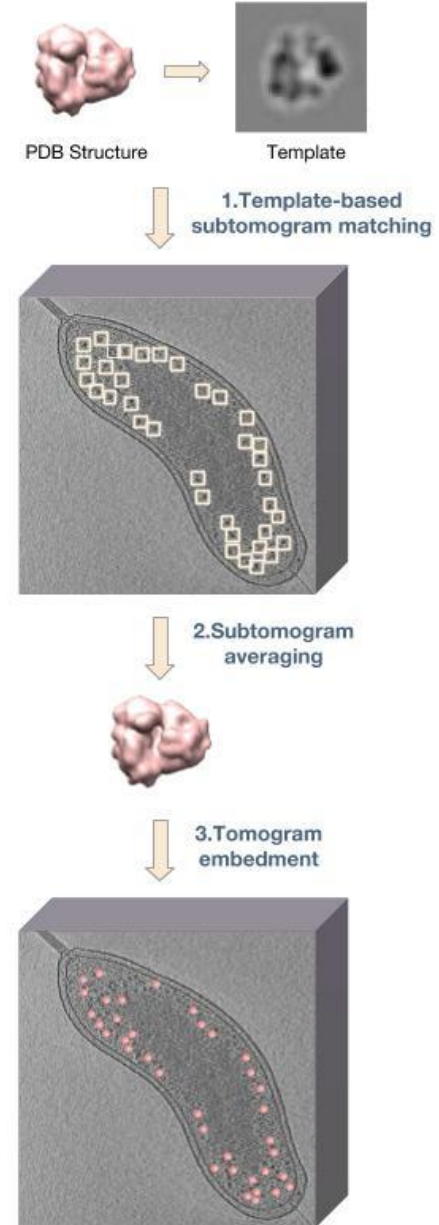
Challenges 4: Molecular crowding



Standard template-based structure recovery pipeline

Drawbacks

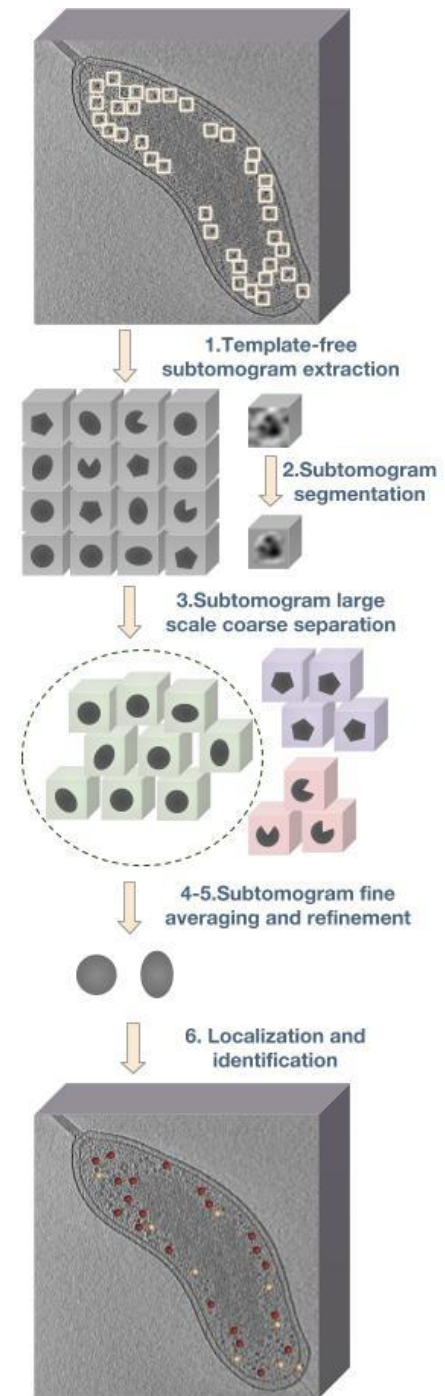
1. Rely on prior knowledge, unable to detect novel structures
2. Could be biased
3. Unsystematic for large datasets



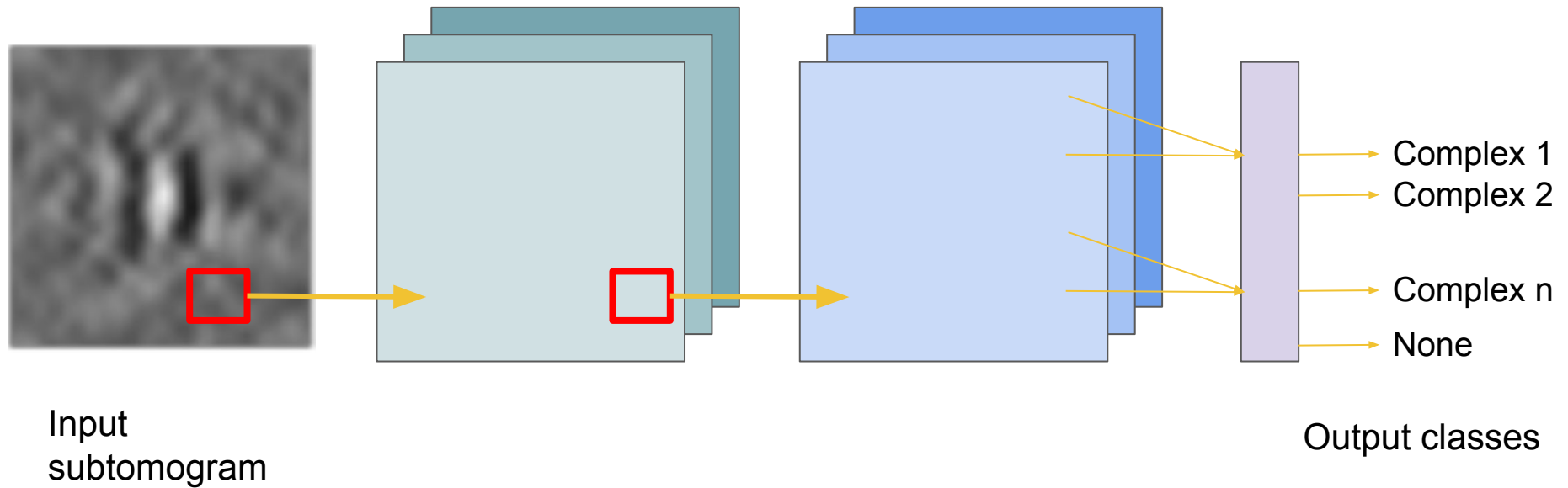
A template-free pipeline

Overview of techniques we developed

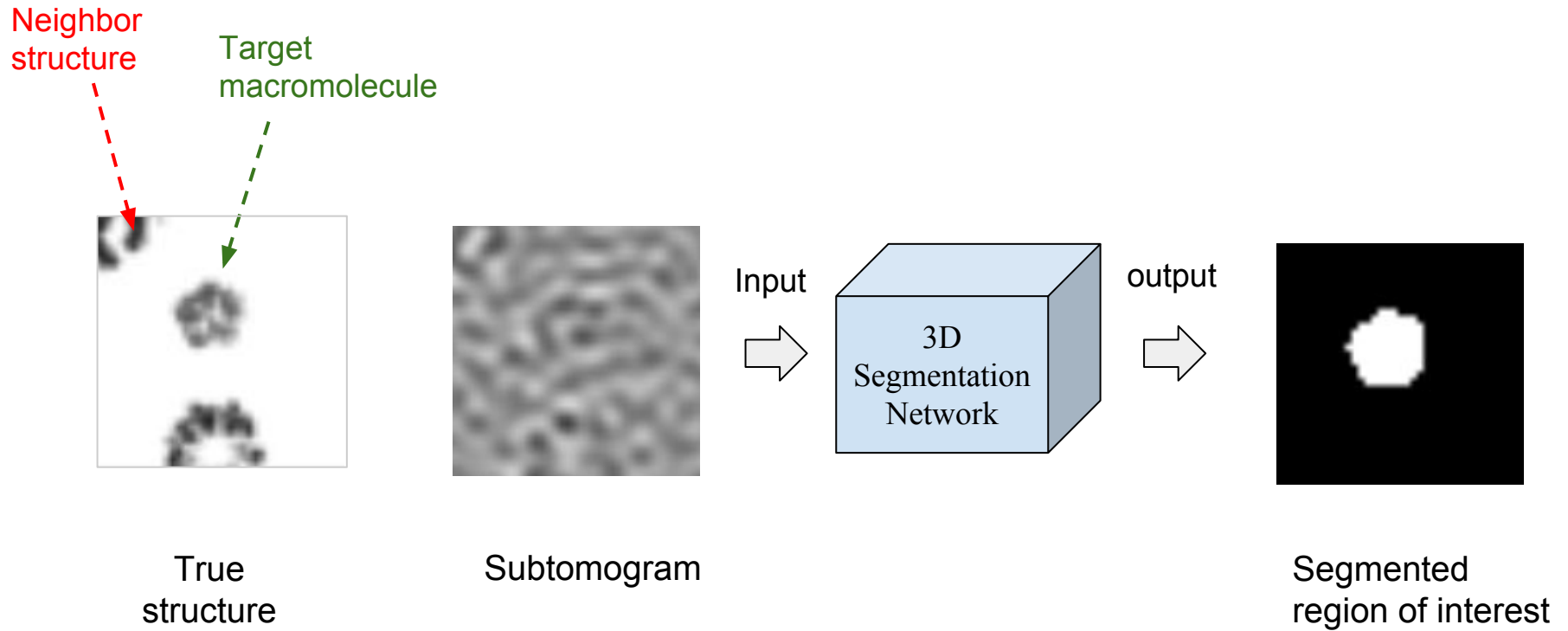
- Subtomogram segmentation
 - Semantic segmentation
- Coarse structural separation
 - Pose normalization
 - Deep structural feature extraction
 - Convolutional Autoencoder
 - CNN classifier
 - Deeper models
 - Model compression
- Averaging and classification
 - Fast alignment + maximum likelihood averaging
- Others
 - Saliency detection
 - Generative models of pseudo molecular structures
 - Multi-task learning



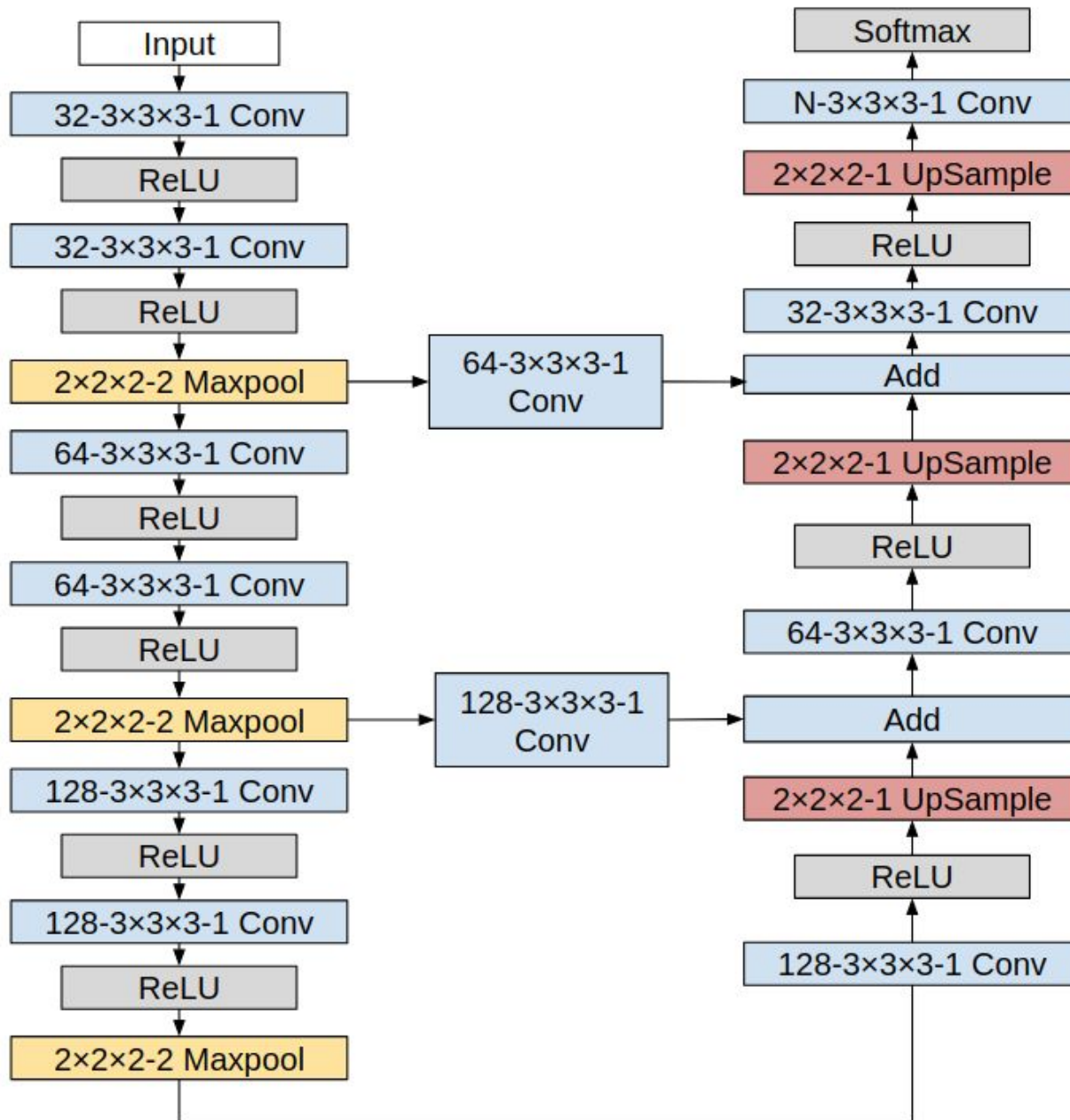
CNN based subtomogram classification



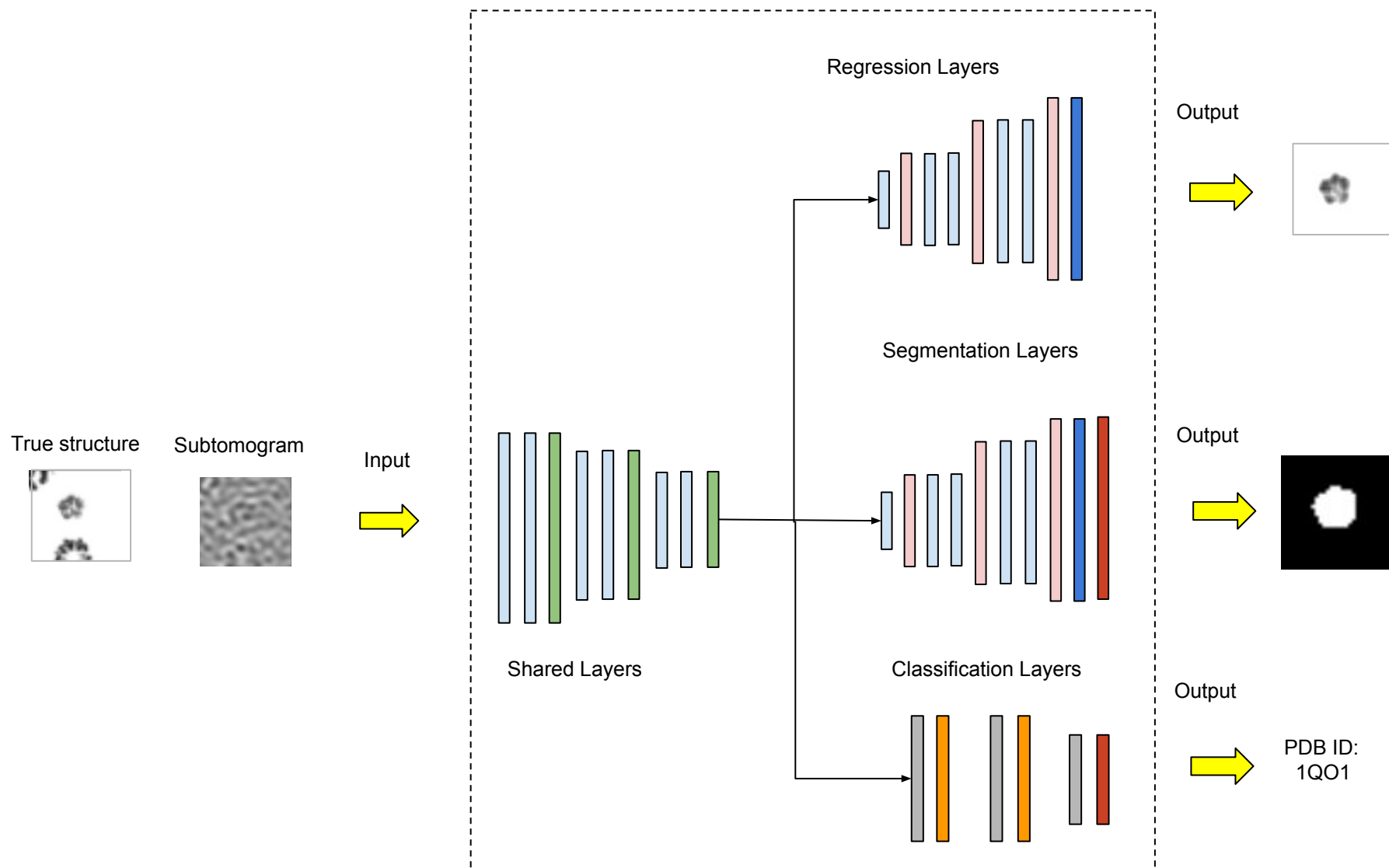
Subtomogram segmentation



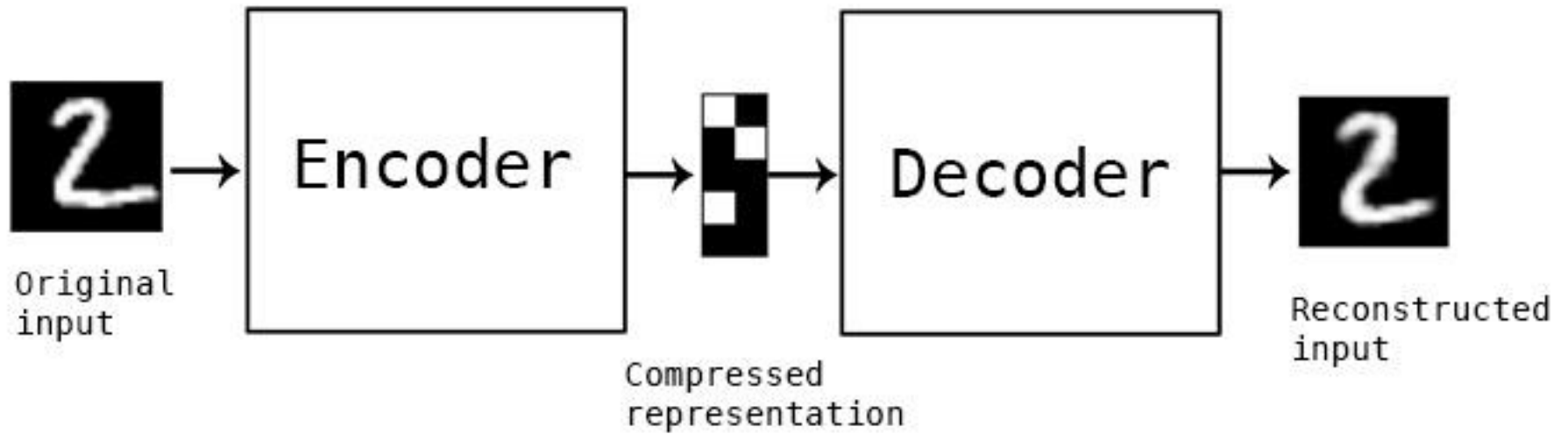
Segmentation network model



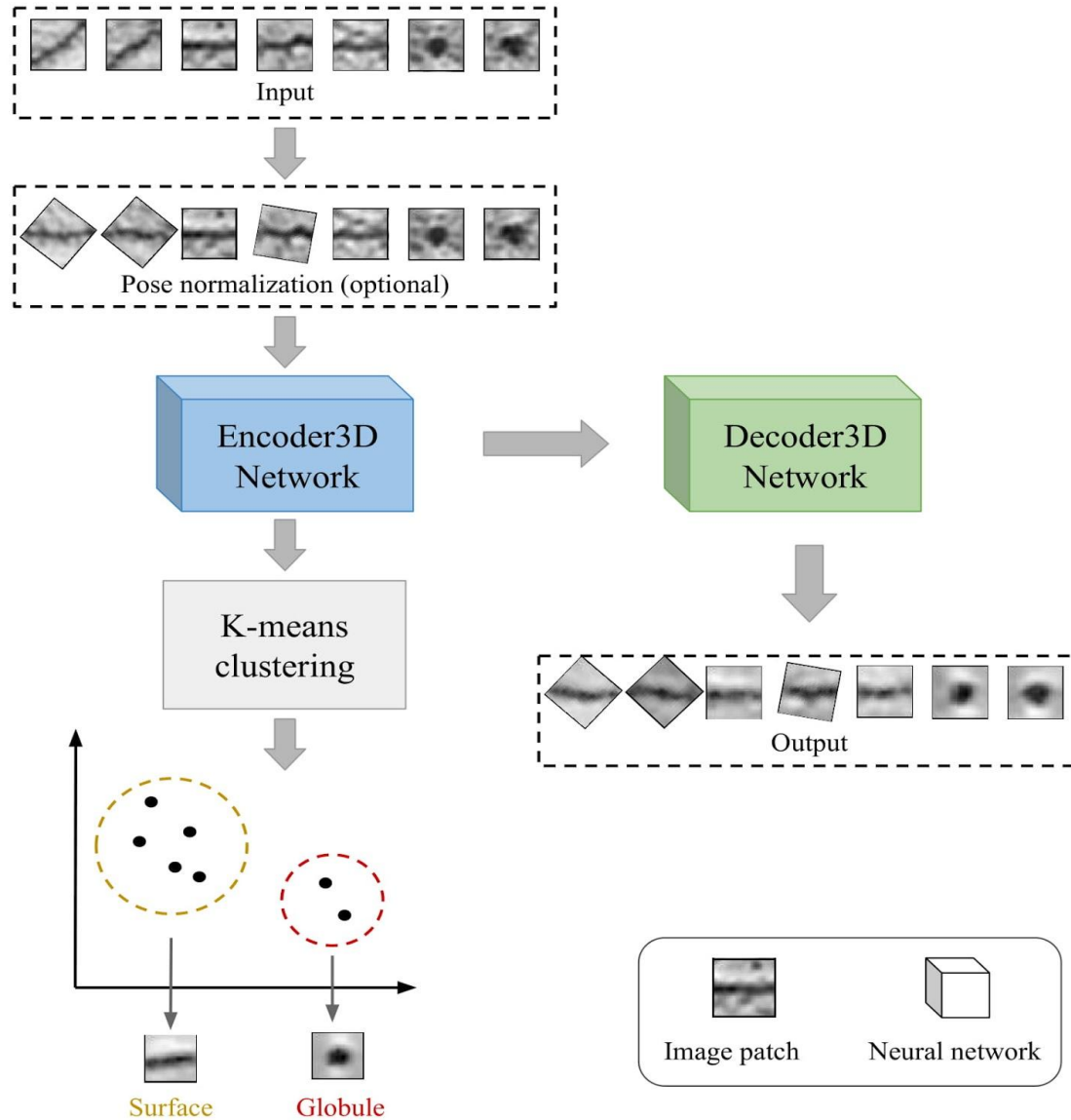
Multi-task learning model



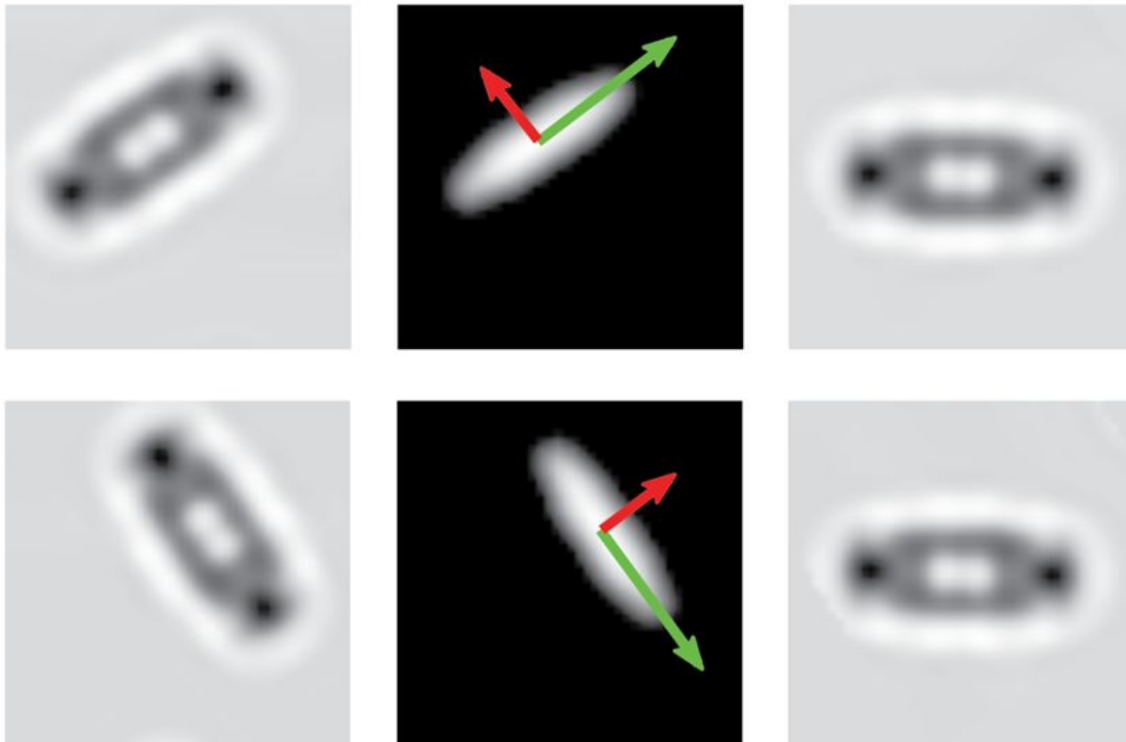
Autoencoder based pattern compression



Autoencoder : large scale subtomogram separation



Pose normalization



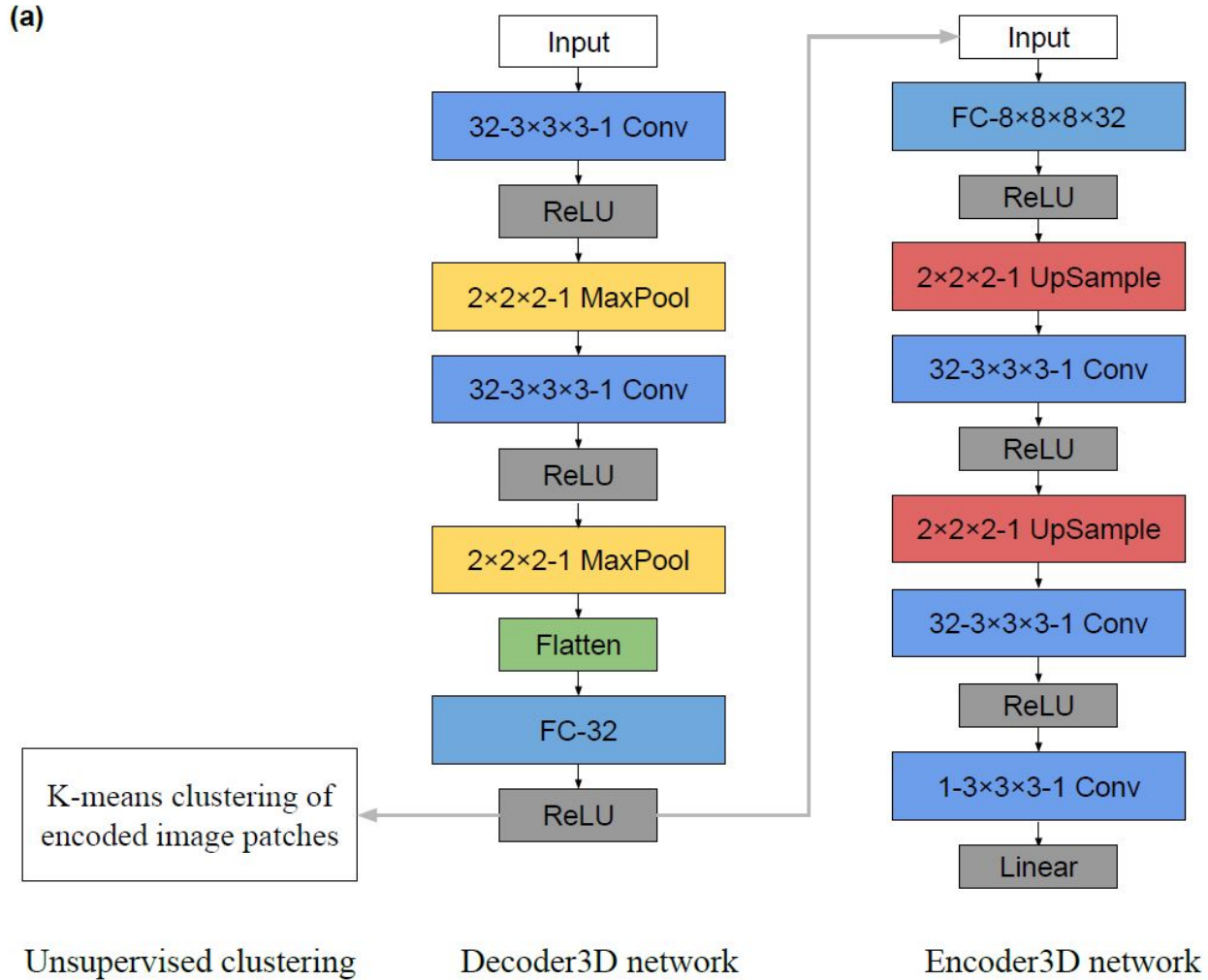
Standard PCA

$$\mathbf{W} = \sum_i \mathbf{X}_i \mathbf{X}_i^\top$$

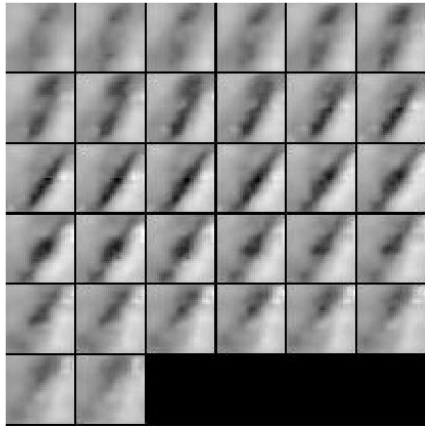
PCA on weighted covariance matrix

$$\mathbf{W} = \int_{\mathbf{x}} \phi(\mathbf{x})^2 \mathbf{x} \mathbf{x}^\top$$

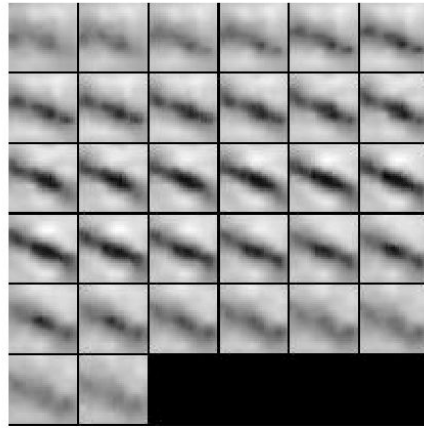
Autoencoder model network



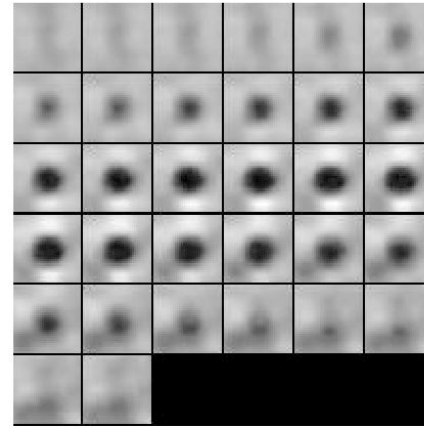
Pattern detected



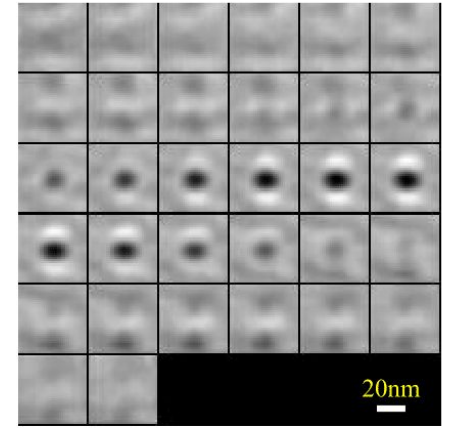
Surface patch



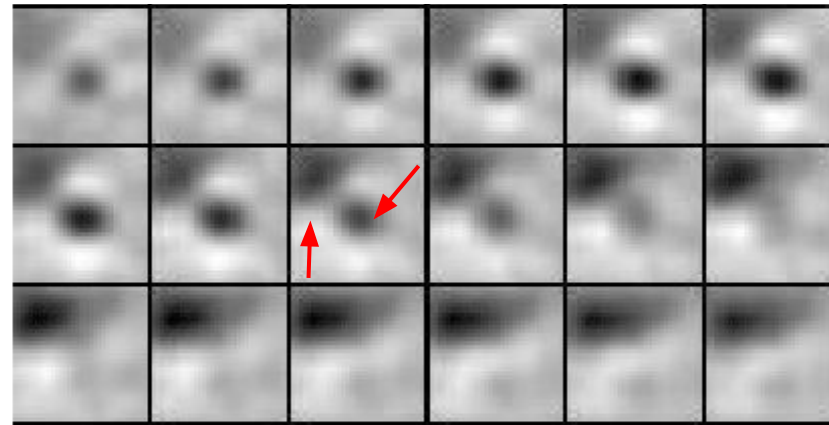
Surface patch



Large globule



Small globule



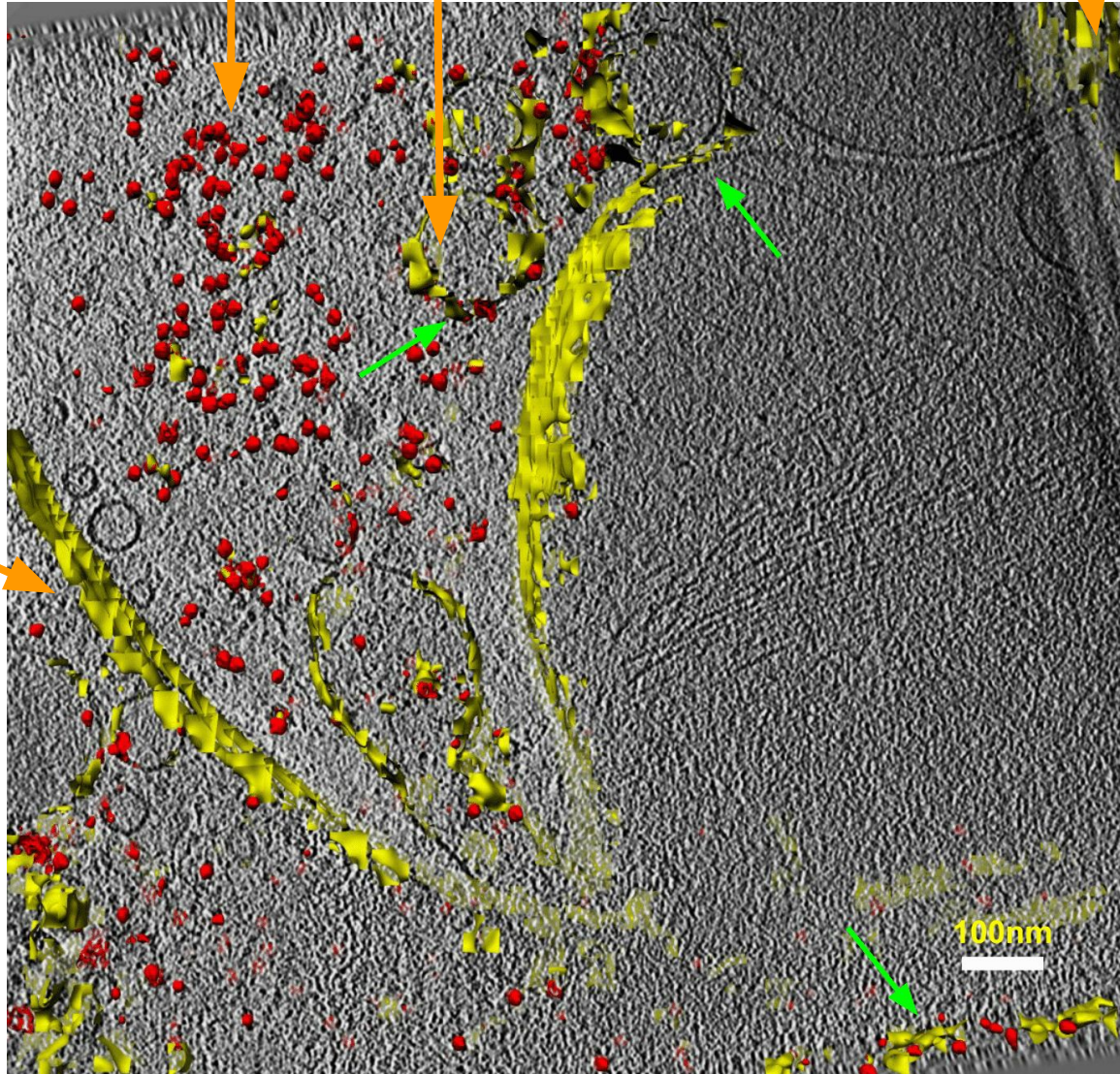
Interaction between cellular components

Pattern embedded

Ribosome like
macromolecule

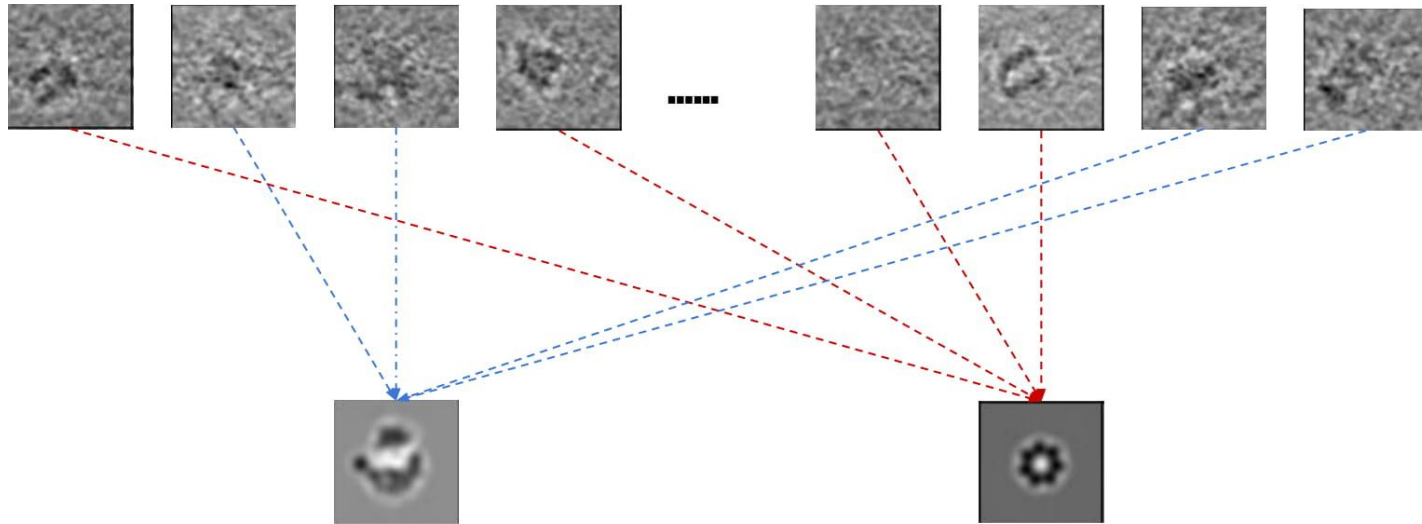
Vesicular
membrane

Tomogram
boundary



Carbon
edge

Subtomogram averaging



N subtomograms are transformed (rotated and translated), clustered, and averaged into K different classes.

Existing method 1 : Maximum likelihood

- Optimizes the probability of observing the data given a data model

$$X_i = R_{\phi_i} A_{\kappa_i} + G_i \quad \forall i = 1, \dots, N$$

- Uses the EM algorithm
- Exhaustive scanning in 6D parametric space of rigid transformation is needed
 - In principle, computationally infeasible

Existing method 2 : Fast alignment

- Optimizes a correlation score between a subtomogram X and an average A :

$$c(\phi^{\text{ro}}, \phi^{\text{tr}}) = \frac{\sum_j w_j^2 X_j \exp(2\pi i \xi_j^\top \phi^{\text{tr}}) \overline{(R_{\phi^{\text{ro}}} A)_j}}{\sqrt{\sum_j w_j^2 [R_{\phi^{\text{ro}}}(A \circ A)]_j}}$$

- Uses the fast rotational matching algorithm
- Searches sub-optimal rigid transformations using local maximum under constraints
- Not sufficiently robust to low SNR and missing wedge effects

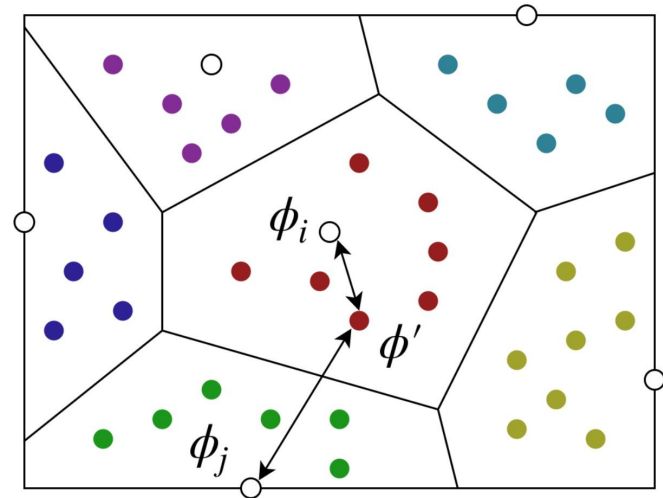
FAML: Integration of two methods

Approximate the integral with sub-optimal transformations:

$$\int_{\phi} f(\phi, X, A) d\phi \approx \sum_{\phi \in \Theta} f(\phi, X, A) \tilde{v}(\phi, \Theta)$$

Where $\tilde{v}(\phi, \Theta) := \frac{|v(\phi, \Theta)|}{\sum_{\phi' \in \Theta} |v(\phi', \Theta)|}$ is the normalized hypervolume of Θ .

Voronoi weights are approximated using Monte-Carlo sampling



FAML: Algorithm

Initialize model parameters $\Theta = (A, \alpha, \sigma, \xi)$ from the distribution of X

For M iterations:

 Compute a list of sub-optimal rigid transformations using FA

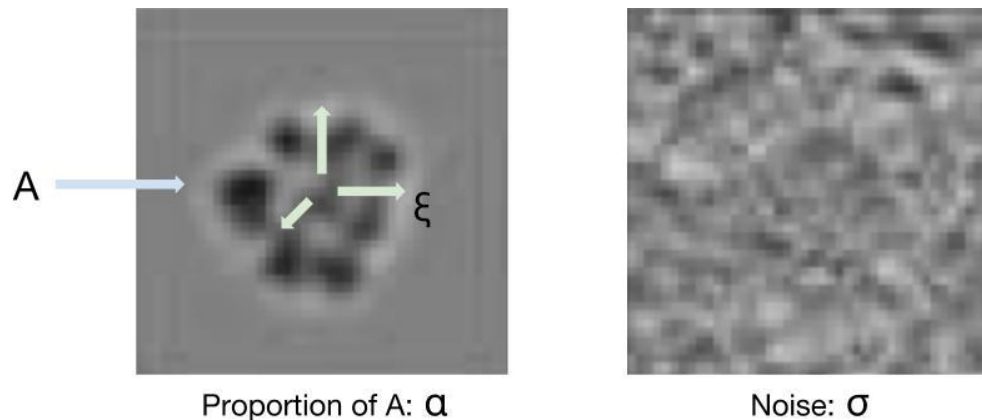
 Compute their Voronoi weights

 Update α , the proportion of particles belonging to different classes

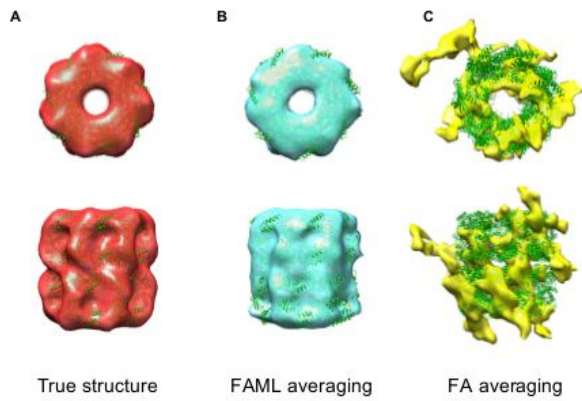
 Update σ , the standard deviation of Gaussian noise

 Update ξ , the standard deviation of translation parameters (3D Gaussian)

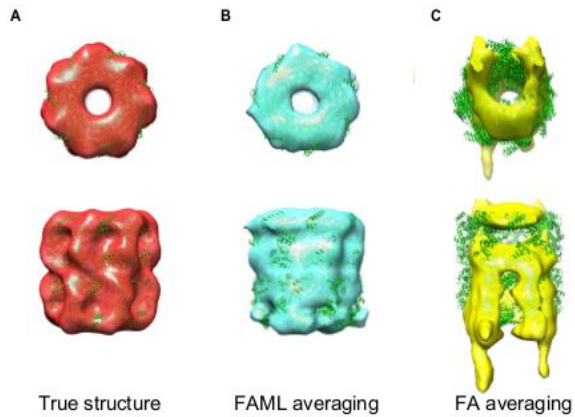
 Update A , the underlying true structure (subtomogram average)



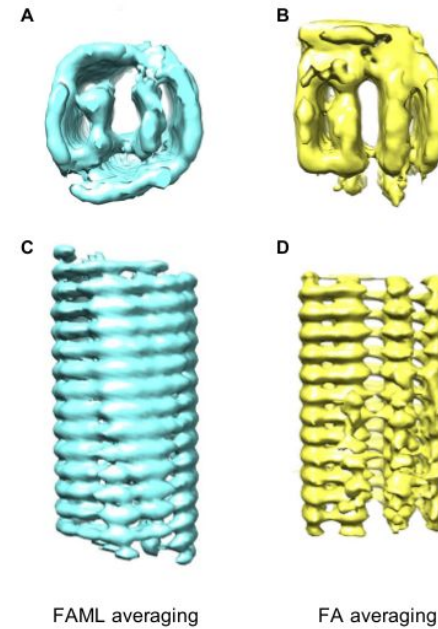
Results



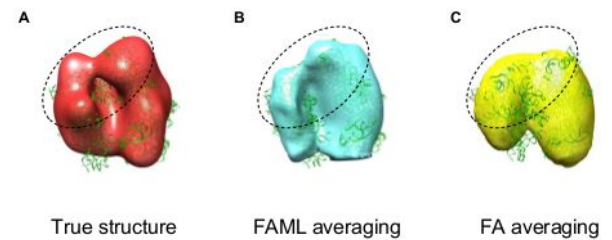
Low SNR



Orientation preferred



TMV (Kunz et al 2015)



Ribosome (Guo et al 2018)

Results

We randomly selected 400 GroEL/GroES subtomograms from an original dataset of 780.

FAML:

GroEL: $r = 0.87$

GroEL-GroES: $r = 0.78$

FA:

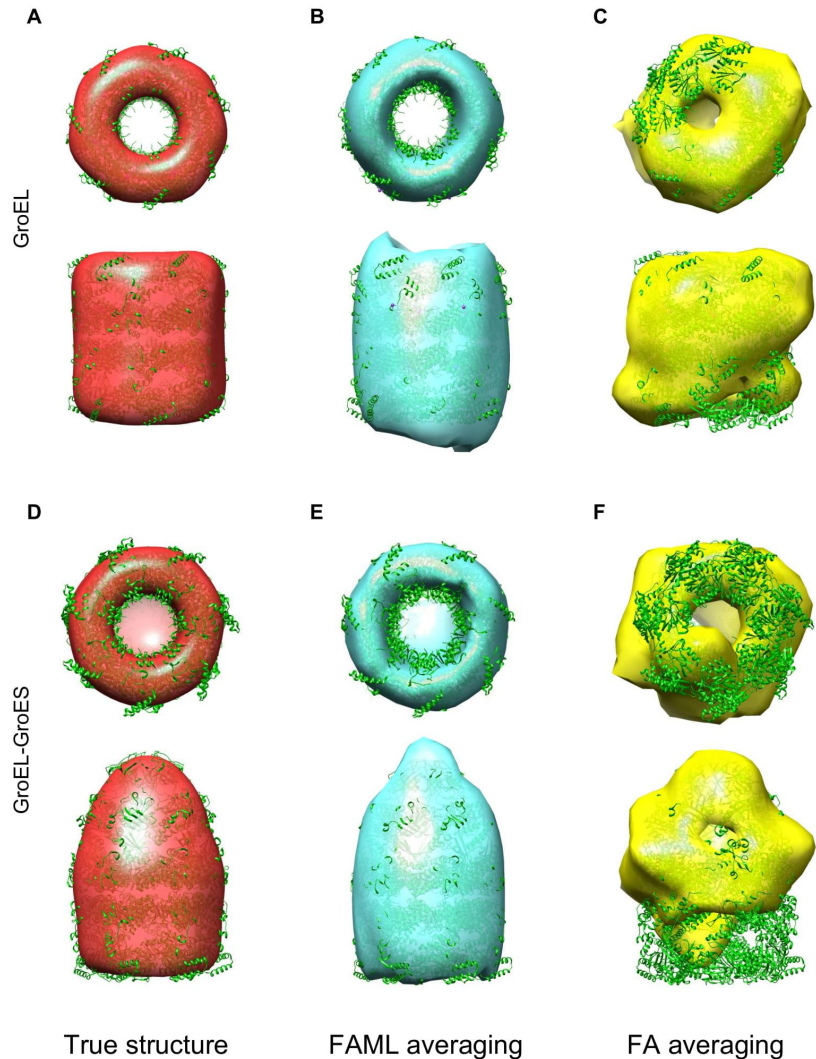
GroEL: $r = 0.40$

GroEL-GroES: $r = 0.24$

ML (on original dataset):

GroEL: $r = 0.88$

GroEL-GroES: $r = 0.81$



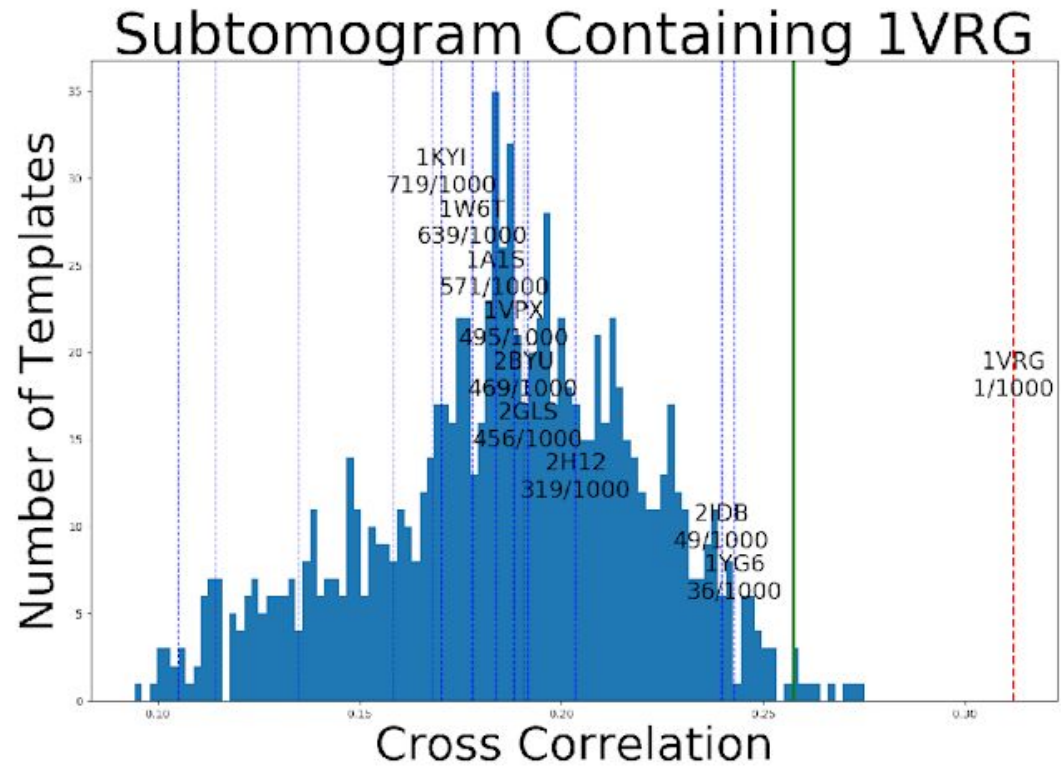
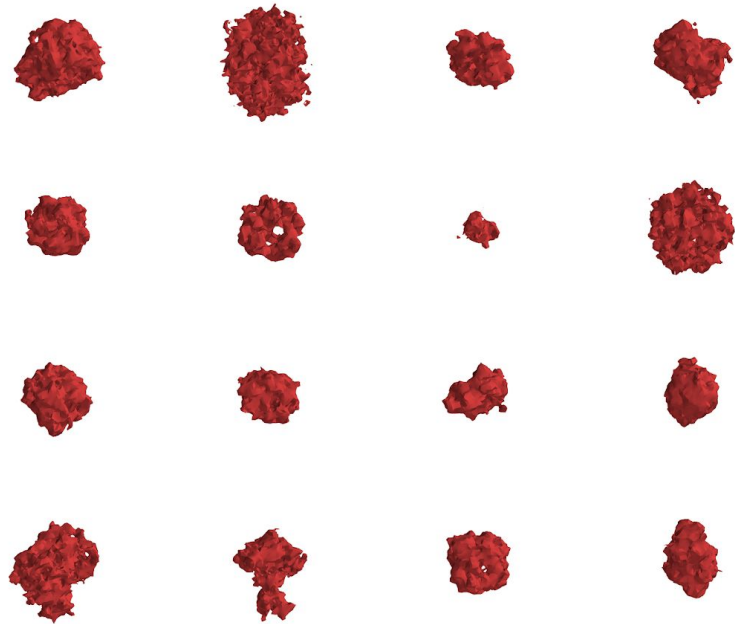
Computing time

Table 1: Computing time used for FA, FAML and RELION methods. 32^3 in parenthesis denotes the testing subtomograms are of size 32^3 .

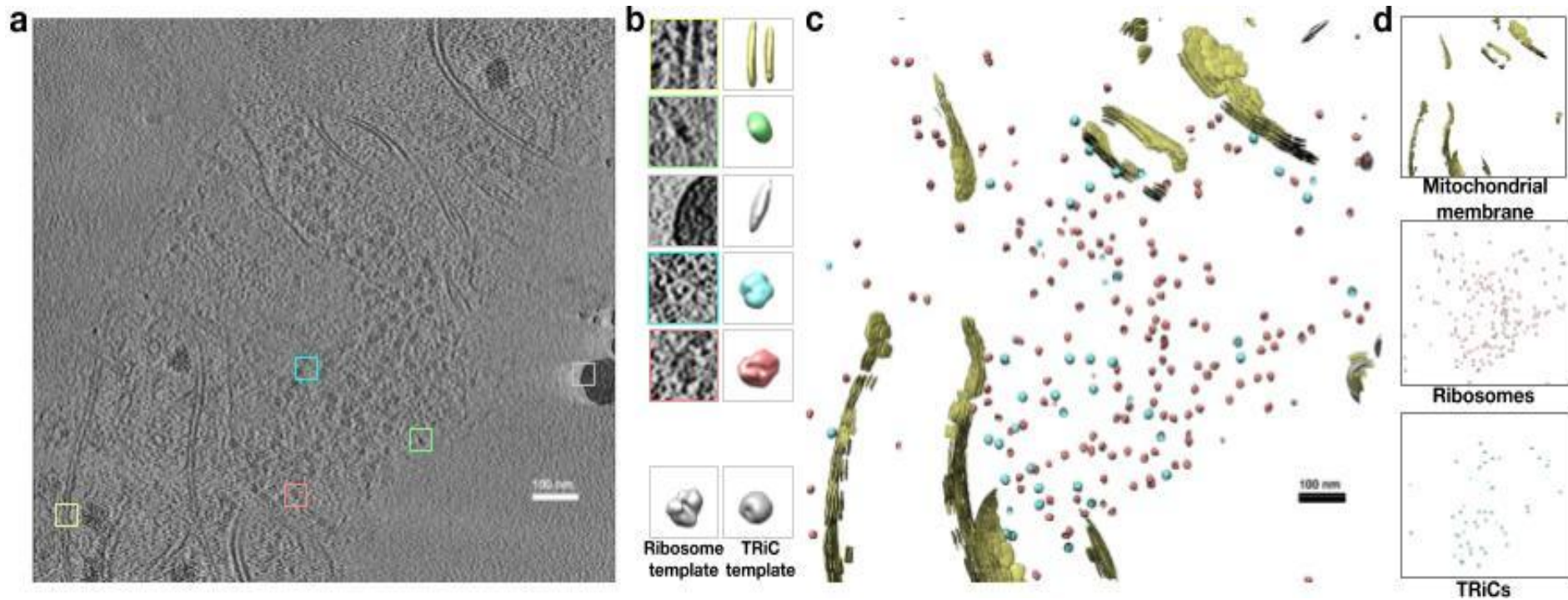
	Iterations to converge	Mean time per iteration	Total time
FA (32^3)	11	7 s	78 s
FAML (32^3)	10	56 s	562 s
RELION (32^3)	8	340 s	2720 s
FA (64^3)	4	27 s	106 s
FAML (64^3)	3	150 s	451 s
RELION (64^3)	6	340 s	2041 s
FA (128^3)	5	143 s	717 s
FAML (128^3)	4	449 s	1794 s
RELION (128^3)	3	921 s	2764 s

- FAML is slower than FA but takes less iterations to converge
- FAML is 2 to 5 times faster than Relion using their default parameters

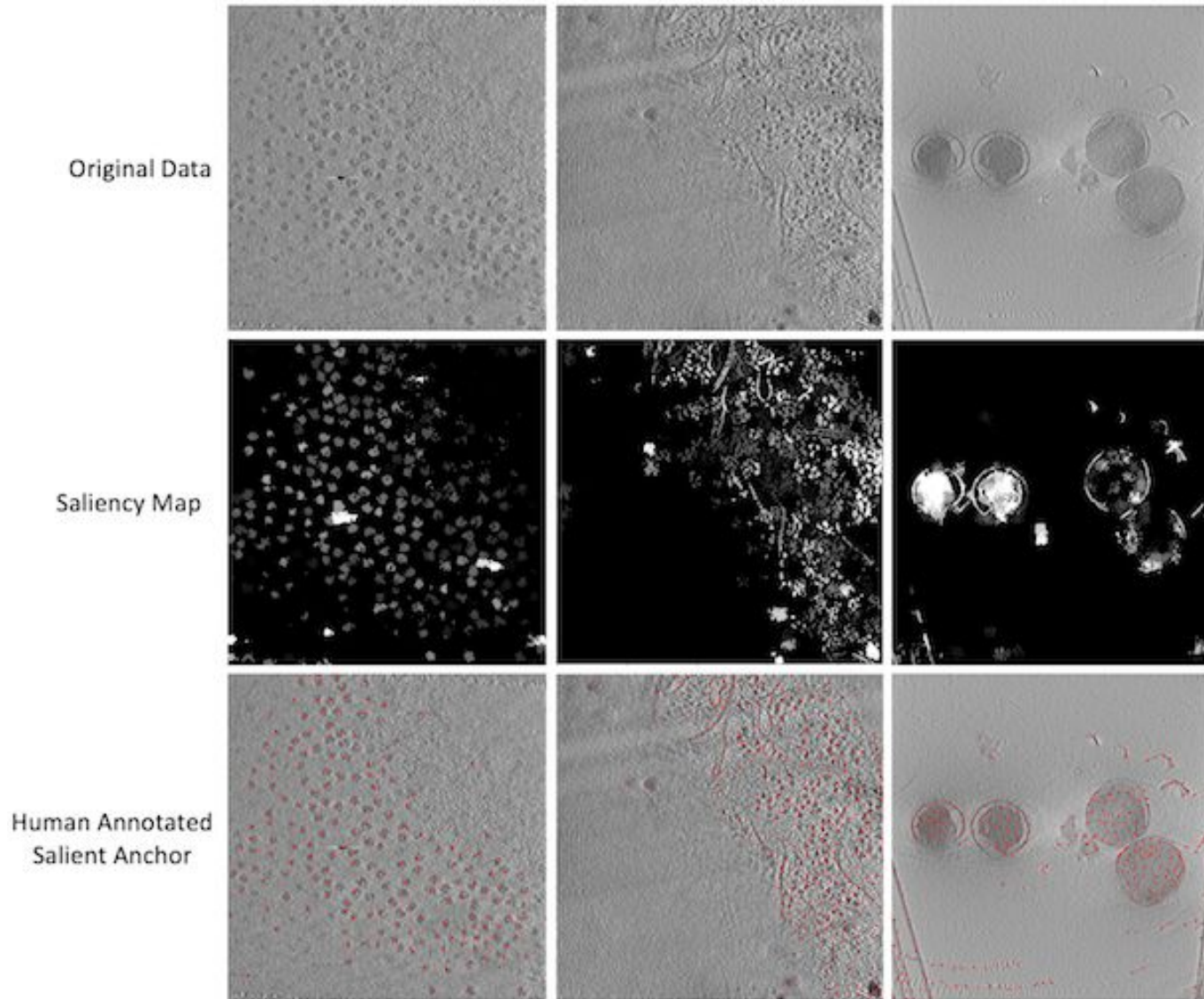
Hypothesis testing for structure identification



Pipeline results on a rat neuron tomogram



Future works



Future works

1. Saliency based particle picking method
2. Better tomogram reconstruction algorithm
3. Fast systematic structure identification method
4. Models for recovered structures
5. Spatial statistical models for macromolecule distribution

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References

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